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1. Introduction

Surface plasmon resonance sensors are one of the types of optical sensors which measure various biologicals and chemical parameters based on the interaction between the sample medium and the sensor surface.[1], [2] To excite surface plasmons at the metal-dielectric interface, the electrons of the metal conduction band must be able to resonance with input light on the surface at a given wavelength.[3]

In surface plasmon resonance based biosensors, gold or silver is generally coated directly onto the prism to separate the sensor medium from the prism. Biomolecules have a low capacity to interact with gold, which reduces the sensitivity of the sensor. To resolve this problem, in recent studies of biosensor structure, one or more layers of graphene have been used because of the high surface-volume ratio, high electrical mobility and stability of the atomic structure.[4] However, it does not act as a semiconductor due to insufficient of bandgap in its electronic structure.[5] This deficiency prevents its use in numerous applications, including optoelectronics. Transitional metal dichalcogenides (TMDs), another important component of the 2D material family, have also aroused scientists' interest. The most common TMDs are molybdenum disulfide (MoS₂), Tungsten disulfide (WS₂), Molybdenum diselenide (MoSe₂) and Tungsten diselenide (WSe₂). They have a perceptible band gap, allowing the conversion of electrons into light photons and resulting in extraordinary on/off ratios. [6]

Today, other 2D materials such as Black phosphorene (BlackP) and Blue phosphorene (BlueP) are being investigated. However, BlackP and BlueP are easily degraded in ambient air.[7] BlueP has the same hexagonal crystalline structure and lattice parameter as TMDs, such as MoS₂, MoSe₂, WS₂ and WSe₂. To avoid the BlueP of external agents, a combination of 2D materials

with BlueP is developed, resulting in the possibility of vander Waals (vdW) heterostructure. Moreover, this heterostructure plays an important role in the improvement of the optical and electronic stability properties of materials compared to their 2D shapes.[8]

In the present article, a structure consisting of different layers of Blue Phosphorene-TMDs (MoS₂, MoSe₂, WS₂, WSe₂) vander Waals (vdW) Heterostructure on an Au layer has been proposed. The structure formed as an SPR biosensor at 633 nm incident light. The various structures were then simulated in the Lumerical environment and modifications of the refractive index were investigated and compared.

2. The Proposed SPR-Biosensor Structure

In this paper, we use the 4-layer Krishmann structure, including the prism, gold (Au) layer, Blue P-TMDs vdW heterostructure, and sample environment, respectively. The physical properties of the different materials used for the simulation are presented in Table I.

Table I. Refractive index and thickness different layers.

Layer	Refractive Index	Thickness
Prism[8]	1.515	-----
Au[8]	0.185+3.423i	30 nm
BP-MoS ₂ [9]	2.81+0.32i	0.75 nm
BP-WS ₂ [9]	2.48+0.17i	0.75 nm
BP-MoSe ₂ [9]	2.77+0.30i	0.75 nm
BP-WSe ₂ [9]	2.0+0.14i	0.75 nm

Important parameters in the surface plasmon resonance sensor that reflect the performance of this sensor include: Sensitivity(S); Indicates the rate of change of sensor output to the measured characteristic changes, expressed as follows.

$$S = \frac{\Delta \theta_{SPR}}{\Delta n} \quad (1)$$

Detection accuracy (D.A) indicates the proximity of the measured characteristic to its true value, and it is mentioned in relation 2.

$$D.A = \frac{\Delta\theta_{SPR}}{FWHM} \quad (2)$$

The quality factor; It is expressed by Equation 3. [10]

$$Q = \frac{S}{FWHM} \quad (3)$$

3. Results and Discussion

The aim of this article is to investigate a new detection configuration with using layers of Blue P-TMDs (MoS₂, WS₂, MoSe₂, WSe₂) on a thin layer of gold to improve the capacity of the light absorption of the SPR-biosensor and to further enhance its sensitivity. As shown in Fig. 1, we first examine the structure with the Au/Blue P-TMDs (1L) sensitive layer and compare it with the results of the gold monolayer at the top of the prism.

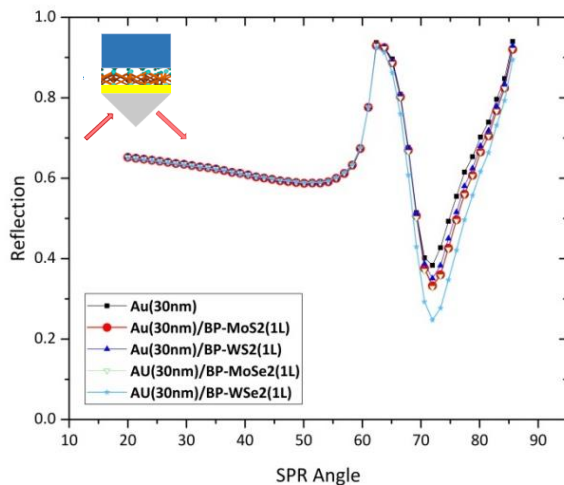


Fig. 1: Illustration of the SPR-biosensor structure

As can be seen in Fig. 1, the minimum reflectance (R_{min}) in the structure with the Au layer and the thickness of 30 nm is 0.247 and by adding an additional monolayer of Blue P-TMDs (MoS₂, WS₂, MoSe₂, WSe₂) on Au a ~30% reduction in R_{min} occurs in 0.247 and an approximate difference in SPR angle is $\Delta\theta \approx 0^\circ$. This is achieved in the best conditions for the Blue P-WSe₂ layer. By retaining the Au layer thickness

at 30 nm, the impact of additional layer of Blue P-WSe₂ on the minimum reflectance of the Au(30 nm)/Blue P-WSe₂ configuration was also investigated and compared. As shown in Fig. 2, when the thickness of Blue P-WSe₂ layer grows the lowest reflectance approaches 0.02 for Au(30 nm)/Blue P-WSe₂(8L). Table II, lists the minimum reflectances corresponding to the angles of occurrence for the setup simulation at different thickness of Blue P-WSe₂ layers in Au30 / Blue P-WSe₂ configurations in $n = 1.33$ environment.

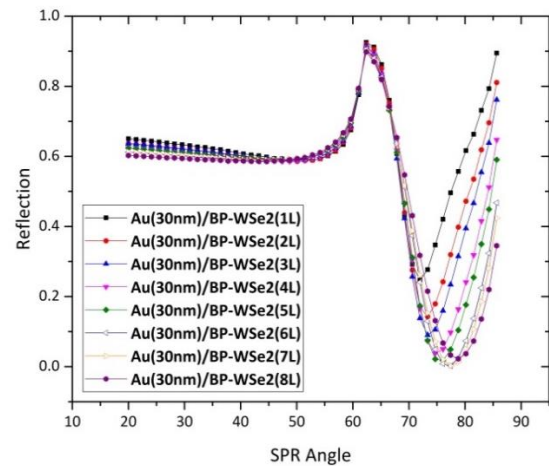


Fig. 2: The reflection spectra for different thickness of Blue P-WSe₂ layers in Au(30 nm)/Blue P-WSe₂

Table II. Resonance angle (θ°) and R_{min} values for different thickness of Blue P-WSe₂ layers in Au30 / Blue P-WSe₂ configurations in $n = 1.33$ environment.

Layer number of Blue P/WSe ₂	Resonance Angle(θ°)	Minimum Reflectance(R_{min})
1	71.90	0.247
2	73.32	0.142
3	73.32	0.090
4	74.69	0.038
5	76.06	0.017
6	77.42	0.002
7	77.42	0.0028
8	78.79	0.002

From the results of Fig. 1 and 2 we can see that the minimum reflectance happens at 0.002. This means that the combination Au(30 nm)/BP-WSe₂(6L) is the most optimal structure among the available configurations. By modifying the

medium to $n = 1.339$, the sensor's sensitivity and the spectral response of the Au(30 nm)/BP- WSe_2 (1 L) structure are investigated. Fig. 3 indicates the response of the spectral reflection to various environments. Sensitivity, can now be determined using the above mentioned Eq. (1) and the details of Fig. 3 for replies to $n = 1.330$ and $n = 1.339$, which are listed in Table III based on Fig. 3 information. The results of another investigation into Au(30 nm)/ G(1 L) are also presented for comparison. [11]

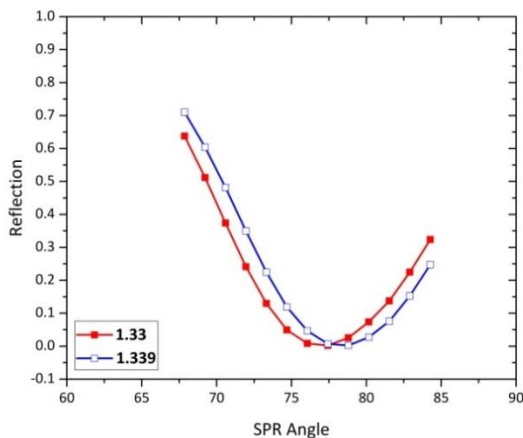


Fig. 3: The reflection spectra for Au(30 nm)/BP- WSe_2 (1 L) configuration at watery ($n = 1.330$) and analyte ($n = 1.339$) representing .

Table III. The sensitivity (S), detection accuracy (DA), and quality (Q) of the proposed Au(30 nm)/BP- WSe_2 (1 L) SPR-biosensor vurses work in [28] for $n = 1.339$ medium.

SPR-Biosensor Configuration	Au(30 nm)/BP- WSe_2 (1 L)	Au(30 nm)/G(1 L)
$FWHM$	10.7	22.06
$\Delta\theta_{SPR}$	1.367	6.20
S (°/RIU)	101.88	89.29
DA	0.887	0.29
Q	9.67	4.26
ref	This work	[11]

4. Conclusion

In this work, the effect of different Au(30 nm)/BP-TMDs(MoS_2 , WS_2 , MoSe_2 , WSe_2) combinations and the number of their flakes on the spectral response of an SPR biosensor was investigated and presented. Moreover, a comparison was made between the structure of layer and the medium. The results indicate that the BP- WSe_2 (1 L) on Au(30 nm) has the highest sensitivity, which is 101.88°/RIU. The results

also show that increasing the thickness of layers in the output has a direct effect on the sensor's efficiency and improves sensor performance.

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